

CONCISE REVIEW

From Finger Taps to Footsteps: Gait as a Model for Investigating and Training Rhythmic Abilities

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ABSTRACT

Synchronization of movements to auditory rhythmic cues, such as music or metronomes, often occurs spontaneously. Nonetheless, important interindividual differences exist in auditory–motor synchronization (AMS). Effects of rhythm on movements are partly modulated by rhythmic abilities, which include beat perception, motor production, and sensorimotor integration. These rhythmic abilities are often assessed using finger-tapping tasks, which can be performed in highly controlled environments and are easy to implement. In this article, we present limitations associated with finger-tapping tasks and propose gait as an alternative model for investigating and training rhythmic abilities. We focus on three key elements that differentiate gait from tapping and are critical in assessing AMS: the need to coordinate multiple effectors, emergent timing associated with continuous actions, and movement automaticity. Interestingly, cued–gait interventions (i.e., walking to rhythmic auditory cues for several weeks) have shown positive effects on all aspects of rhythmic abilities, while tapping interventions (e.g., playing tablet-based serious games) might lead to more limited transfer. In sum, gait offers a functionally rich behavioral model that can capture the complexity and ecological validity necessary to study and train AMS.

1 | Introduction

Synchronizing movements to sound is a natural response in humans. This behavior can be deliberate, as in dancing or clapping along music, or spontaneous, like when we tap our foot or nod our head without thinking during a concert. The beat is a basic characteristic of rhythm in music, and it underlies most pieces. Its temporal regularity makes it predictable. In turn, predictions enable us to coordinate movements to the perceived regularities, such as during speaking, walking, dancing, or playing a musical instrument. The ability to align movements to an auditory beat (auditory–motor synchronization, AMS) arises early in life [1, 2] and is widespread in the general population [3, 4]. Difficulties in AMS have been linked to neurodevelopmental [5–8] and neurodegenerative disorders [9, 10]. Interestingly, patients with motor disorders such as Parkinson’s disease can

benefit from rhythmic auditory cues (for reviews, see Refs. [11, 12]). Gait improvements such as reduced variability, increased speed, and increased stride length are well documented in these patients [13–16].

These effects of rhythm on movement may be possible due to the tight link between auditory and motor areas in the brain [17–19] (for a recent review, see Ref. [20]). When listening to an auditory beat (in the absence of movement), a broad neural network including auditory regions, motor regions, and sensorimotor integration areas is activated. It is no surprise that areas associated with audition such as the superior temporal gyrus are active during listening tasks. More surprisingly is the activation of the supplementary motor area, basal ganglia and cerebellum [17, 21–23], typically known for their role in motor control and action planning in the absence of external rhythmic stimulation

[24–26]. While the basal ganglia (e.g., the putamen) appears central in beat processing, areas like the supplementary motor area and the cerebellum are particularly active for perceiving complex rhythms [27]. Cortical and subcortical regions involved in beat perception are thus overlapping with those involved in action planning and production. A theory accounting for the tight link between perception and action is the Action Simulation for Auditory Prediction (ASAP) hypothesis, which postulates that the internal (unconscious) simulation of movements by motor areas enables precise temporal predictions of the upcoming stimulus [28, 29]. In turn, these predictive abilities improve auditory processing [30] and thus, beat perception, which is necessary for AMS [16, 31].

AMS can be modeled using different approaches. Computational models, such as the Wing and Kristofferson [32] model, distinguish two key components in rhythmic movement production: an internal clock underlying spontaneous movement rate, and a motor implementation process that introduces delays to produce the actual movement. During AMS, sensorimotor delays must be compensated to reach a synchronized state. Such compensation happens through implementation of phase and period adjustments [33, 34]. Another approach for understanding AMS derives from the dynamical system theory. In this framework, movements and auditory cues are modeled by two distinct oscillators, which both have their own preferred frequency. Spontaneous movement rate (e.g., uncued step cadence for walking) defines the preferred frequency of the movement oscillator, while the beat of the auditory stimulus constitutes the frequency of the other oscillator. The distance between the oscillators' frequencies defines the synchronization region where coupling (i.e., synchronization) is possible. For coupling to occur, the two frequencies must be sufficiently close [35, 36] or their ratio be close to an integer ratio [37]. The larger the synchronization region, the greater the coupling strength. If the stimulus' frequency is too far from the spontaneous motor frequency, however, synchronization may suffer [35]. An influential model of rhythm perception—the dynamic attending theory [38, 39]—builds on dynamical system theory. According to the dynamic attending theory, temporal predictions, which are critical for achieving AMS, derive from the coupling of internal neurocognitive oscillations [40–42] reflecting attending mechanisms to rhythmic auditory stimuli. Indeed, attention oscillates through time, and attentional energy is expected to be maximal whenever a sensory event is most likely to occur. For example, the metrical structure typically found in music leads to the perception of an underlying beat or pulse, while driving strong expectations for sensory events (e.g., notes, chords) to fall on the beat. When notes occur in-between beats, as is the case in syncopated rhythms, temporal expectations are violated [43] leading to prediction errors. In the predictive coding theory [44, 45], the brain aims to minimize prediction errors by adjusting internal models until predictions match sensory input. When we dance to syncopated rhythms, we typically move to the beat of music, thus minimizing prediction errors [44]. Together, these models highlight the interplay between intrinsic motor rhythms, external auditory cues, and attention, offering a comprehensive framework for understanding the mechanisms underlying AMS.

In sum, different theories can model the processes and brain mechanisms underlying AMS. In addition to these general mechanisms, a critical element to achieve AMS pertains to an

individual's ability to track the beat and coordinate motor activity leading to synchronization.

2 | Rhythmic Abilities

Rhythmic abilities encompass beat perception, motor production, as well as sensorimotor integration. Beat perception is the ability to extract the beat from an auditory sequence without overt movement, while motor production refers to the production of rhythmic movements whether a pacing stimulus is present or not. Finally, sensorimotor integration is the process where stimulus timing is mapped onto action timing during planning, eventually leading to precise AMS. These abilities are tested with a variety of perceptual and production tasks, such as the beat alignment test (BAT) [46], and paced and unpaced finger tapping [36]. A very common model to test AMS and motor performance is finger tapping [36, 47]. Test batteries such as the Harvard Beat Alignment Test (H-BAT) [48] and the Battery for the Assessment of Auditory Sensorimotor and Timing Abilities (BAASTA) [4] have been devised to provide a systematic assessment of rhythmic abilities. For example, tasks taken from BAASTA are capable of characterizing individual differences in both musicians and nonmusicians. Notably, adult norms for BAASTA were published for the first time by Dalla Bella et al., providing a reference point for its application to clinical populations [4].

Studies in quite large cohorts generally reveal a link between rhythm perception (e.g., tested with the BAT) and AMS [49, 50]. These relationships point to a general rhythm system, supporting both perception and action—a view which is compatible with the ASAP theory [28, 29]. The idea of a general rhythm system is supported by clinical studies in patients with movement disorders [51]. In Parkinson's disease, movement velocity [52] and variability [53] show cross-effector correlations when performing rhythmic tasks such as tapping, walking, and speaking. Motor variability can further be predicted by patients' beat perception [53]. Finally, there is evidence that training AMS in this population can improve motor performance across different effectors, a benefit linked to improved beat perception [54]. In the context of rehabilitation, having a generalized rhythm system is of interest as patients can gain cross-effector benefits from training a single effector [54].

Although individuals with neurodevelopmental [5–8] and neurodegenerative disorders [9, 10, 55] show deficits in rhythmic abilities, they can also be selectively impaired in perception or production. In fact, some studies report a lack of relationship between beat perception and AMS in healthy and clinical populations [3, 4, 48, 56–59]. This suggests, that even though rhythm perception and production are tightly coupled, there may still be some degree of independence at the functional level, and that the underlying mechanisms may be dissociated in populations with disorders. Moreover, there is preliminary evidence in patients with Parkinson's disease that rhythmic training via finger tapping can transfer to verbal production (i.e., by reducing motor variability when repeating syllables in a loop as fast as possible), but not to walking, as interstep interval variability remains similar post intervention [54]. Thus, timing-control mechanisms may differ for tapping (a minimal motor task) and walking (a full-body task), raising the question of whether assessing motor production

and sensorimotor integration with finger-tapping tasks suffices to gain a good understanding of one's rhythmic profile.

Notably, finger tapping as a model for testing AMS has many advantages. It is easy to implement both in laboratory and clinical settings as it requires minimal equipment, such as general MIDI instruments or off-the-shelf mobile devices [49, 60]. Tapping can also be tested in a brain-imaging scanner to investigate the neural correlates of rhythmic abilities [21]. At the same time, finger tapping presents several drawbacks. It is not an ecological task and may thus limit our understanding of AMS and its underlying mechanisms. Indeed, conclusions drawn from highly controlled tapping experiments may not transfer fully to everyday-life situations, like walking or speaking. For example, walking requires the coordination of multiple effectors and is mostly automatic, while tapping is primarily voluntary and engages only one effector with limited constraints. There are also no consequences in producing unequal finger taps, while unstable gait predicts falls [61]. Walking or speech articulation have clear functional roles, which are absent from tapping. Assessing finger tapping alone may thus not give a full picture of an individual's rhythmic profile.

The aim of this article is to propose gait as an alternative behavioral model for studying AMS. Walking is an inherently rhythmic behavior, as is visible in the regularity of the gait cycle, with high ecological validity. It is rooted in biology as an evolutionary trait, which was acquired over 4 million years ago by our ancestors, as a response to critical environmental pressures linked to changing habitat and a need for efficient harvest [62, 63]. Bipedalism was also paramount in the evolution of other human traits, like speech [64]. Moving from a quadrupedal to an upright position freed the thorax from its support role, leading to the formation of the modern vocal tract and uncoupling of breathing from locomotor functions, a necessity for speech production [64, 65]. Gait emerges spontaneously within the first year of life and follows a regular development in children. We usually can walk at age one, and reach a gait pattern similar to adults' by age seven [66]. Although walking is mostly automatic, it remains under voluntary control for initiation, termination, turning, and obstacle avoidance [67]. Unlike tapping, gait also has a clear functional role. Locomotion is subjected to environmental constraints and requires the coordination of all limbs for the body to stay upright. Loss of coordination may compromise balance, leading to falls and injuries [68]. Altogether, gait offers an evolutionarily grounded and functionally rich behavioral model that can capture the complexity and ecological validity necessary to study AMS.

3 | Walking as a Model of Auditory–Motor Synchronization

3.1 | Single-Effect Versus Whole-Body Movements

When walking to an auditory beat, the alignment of footfalls to the rhythmic stimulus is obviously more complex than for finger tapping, as gait requires whole-body movements and interlimb coordination. Accurately aligning steps to a pacing stimulus irrespective of the movements of other effectors would lead to an unnatural gait pattern. As such, gait analysis requires taking into account all parts of the lower limbs simultaneously

[69, 70]. Analyses assessing effects of a pacing stimulus on gait often focus on spatiotemporal parameters (Figure 1) like gait velocity, cadence (i.e., number of steps per minute), stride length, and variability of interstep intervals and of stride lengths [71]. More rarely, lower-limb kinematics (e.g., joint angles) and kinetics (e.g., joint moments) are also assessed [72–74]. All of these gait parameters are very much affected by gait speed [75]. Speed is determined by cadence and stride length, which are most often targeted by rhythm interventions [76, 77]. Because deviating from gait preferred frequency will impact all effectors up the kinematic chain, the choice of pacing frequency should be carefully considered. Conversely, in tapping, changes in the finger's rate and/or trajectory should not affect other limbs. In sum, AMS during gait involves complex whole-body coordination unlike finger tapping, requiring a comprehensive analysis of spatiotemporal and biomechanical parameters.

The coordination of multiple effectors is likely to rely on timing-control mechanisms that differ from those needed to produce regular finger taps. Alternatively, evidence of a link between tapping and walking performance would suggest similar mechanisms, in favor of a generalized rhythm system. At the moment, there is conflicting evidence regarding the existence of such a link. Indeed, previous studies attempted to predict rhythm-induced gait changes, based on participants' rhythmic abilities assessed with finger tapping [10, 78]. In patients with Parkinson's disease, poor AMS during tapping predicts an increase in gait speed following a cued–gait intervention [10]. AMS however does not seem to predict motor variability during gait in a sample of Parkinson's patients and controls [78]. One could argue that these null relationships stem from the comparison of motor production measures (e.g., variability of interstep intervals) to AMS variables. However, intertap interval variability was not correlated to interstep interval variability after a 6-week rhythm intervention [54]. Interlimb coordination, which is absent from tapping but inherent to gait, could be the source of the discrepancy. Altogether, it is unlikely that tapping performance can fully predict gait adaptation to rhythmic auditory cues, although more research directly comparing the two is needed.

3.2 | Discrete Versus Continuous Movements

Discrete movements are defined by salient events interspersed by breaks [79]. During tapping, finger velocity reaches zero when finishing its downward trajectory and then changes direction before reaching zero again at the apex. On the other hand, walking is defined as continuous, as there are no breaks in the motion until the task is stopped. Timing-control mechanisms of discrete and continuous movements have been compared in the past using the dual-task paradigm [80, 81]. In the present review, we consider dual-task paradigms that involve performing a primary motor task together with a secondary task that can be motor [81], cognitive [80], or both (i.e., name digits presented two cycles ago in an N-back task) [82]. The performance of the secondary task interferes with the primary task by increasing cognitive load. Interestingly, interference is not the same when the primary task is discrete or continuous. For example, when asked to perform a simultaneous working memory task, cellists' variability increases for discrete (i.e., staccato), but not continuous (i.e., legato) upper-limb bowing movements [80]. Here, the cognitive task only

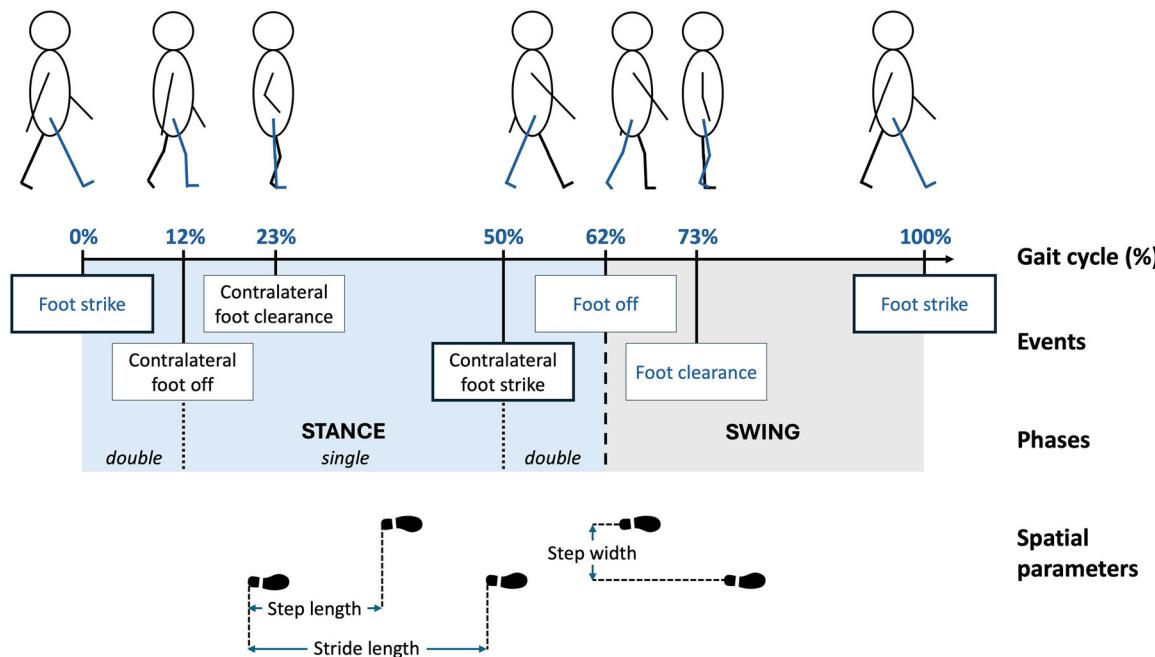


FIGURE 1 | The gait cycle expressed in percentages. Gait events, phases, and spatial parameters are expressed for the right leg (in blue).

interferes with the discrete, but not the continuous motor task. Similar results are observed while performing two competing motor tasks, namely, tapping and walking. Indeed, young healthy adults can maintain a 375-ms tapping rate independently of a 600-ms walking rate [81]. However, if stepping becomes a discrete task (i.e., unilateral or bilateral foot tapping), finger-tapping rate increases to reach a 2:1 ratio with stepping rate. Thus, a discrete task cannot be performed independently of another discrete motor task or a purely cognitive task. Overall, the results indicate that discrete movements require more cognitive resources than continuous ones.

It has been proposed that temporal regularity of discrete movements relies on a pacemaker (i.e., internal clock) [83]. According to clock models, pulses generated by the pacemaker are stored in working memory and compared to timing of discrete events [84]. Error correction thus happens for each repetition. On the other hand, continuous movements would rely on emergent timing, which arises from movement dynamics [85, 86]. At 2 Hz and above, flexion-extension of the finger becomes a continuous movement, as motion breaks are no longer observed in the finger trajectory [86]. This may explain the tendency to speed up discrete actions during simultaneous performance of a cognitive task [80, 82]. By increasing movement rate, action timing may become more dynamically driven, freeing up cognitive resources. These resources can then be allocated to the cognitive task in a dual-task paradigm.

This speeding-up advantage goes against the view of dynamical systems theory, which predicts a loss of stability at increased tempi [87]. Torre and Balasubramaniam [88] proposed that clock models, such as the Wing and Kristofferson [32] model, and dynamical systems could explain the differences observed between discrete and continuous movements during AMS, respectively. Negative lag 1 autocorrelations (i.e., shortened intervals are followed by lengthened ones and vice versa) measured

when finger tapping on a surface show that error correction happens on each repetition, while the lack of negative lag 1 autocorrelations for continuous movements imply that action timing is adjusted continuously as proposed by dynamical systems [89].

Intuitively, we would expect the simultaneous performance of two continuous movements to be unchallenging, if timing can be dynamically driven. In two studies [90, 91], Sakamoto et al. showed that leg cycling rate affected arm cycling rate but that arm cycling rate did not impact leg cycling rate. These studies suggest that there could be a difference between upper- and lower-limb rhythmic motion, despite both movements being continuous. Similar observations are made when looking at AMS. Participants are better at matching metronome tempo during foot stepping than hand circle drawing, despite foot stepping being a discrete motion [92]. Further, synchronization can be maintained when stepping in place regardless of tempo, while synchronization during circle-drawing is negatively impacted by faster pacing stimuli. Despite these results, it is unlikely that differences between upper- and lower-limb rhythmic motion are effector driven. Indeed, we mentioned previously that rhythmic tapping with the finger could only be maintained while walking, but not foot tapping. This discrepancy could be due to the discrete nature of foot tapping, but also to gait automaticity. In sum, different timing-control mechanisms are at play when performing discrete and continuous movements. These differences are likely to be relevant when assessing AMS.

3.3 | Voluntary Versus Automatic Movements

One could argue that highly trained musicians are experts at finger tapping, which resembles piano keystrokes and left-hand motion of guitar and other string players. Indeed, instrumentalists often perform better on rhythm production tasks than nonmusicians [4, 93–96]. For example, Tranchant et al. [97]

reported intertap intervals with ~5% variability in musicians and with ~6% variability in nonmusicians, similar to values reported in BAASTA norms [49]. As for walking, most of us become experts during childhood [66]. Interestingly, and in spite of walking being a more complex multilimb task than tapping, variability of interstep intervals during gait for young [31] and older individuals [98] is twice lower than values of intertap interval variability in musicians [49, 97]. The level of stability achieved during gait may be due to its automaticity.

Gait automaticity is possible owing to its reliance on specific neural structures. Gait recruits both spinal and supraspinal neural networks [99]. The automatic component of gait is implemented by central pattern generators located in the inferior part of the spinal cord, which ensure repetitiveness of the gait cycle and alternating left-right movements at a regular pace when further monitoring is not needed [100–102]. Gait being autonomous, stable, and inherently rhythmic, it is often modeled as an inverted pendulum [103], which makes it an ideal behavior to be studied under the lens of dynamical systems [104]. As an oscillator, gait has an intrinsic frequency with little interindividual variability [105] compared to tapping [106]. As predicted by dynamical systems [107], coupling to an external oscillator (e.g., rhythmic auditory cues) during gait is possible if the external frequency is close enough to spontaneous cadence [35]. Importantly, the level of automaticity achieved through central pattern generators explains why we can walk while successfully performing other tasks [81]. On the other hand, voluntary control is afforded by cortical and subcortical structures receiving feedback from central pattern generators and whose functions allow us to initiate, stop, and change directions, making gait flexible and adaptable to varying environmental demands [99, 100, 108, 109]. Notably, finger or foot tapping lack the aforementioned automatic component. As a result, cognitive resources must be shared when these actions are performed together with a secondary task [82], leading to greater interference than in a walking task [81].

Overall, the studies reviewed in this section suggest a dissociation between tapping, which relies mostly on supraspinal structures, and walking, which is both automatic and voluntary due to the involvement of central pattern generators and cortical and subcortical structures, respectively. As it is possible to manipulate the degree of automaticity required to complete a gait task (e.g., walking on a pressure mat in a lab vs. around a university campus), gait offers the possibility of studying both voluntary and automatic components during AMS.

In conclusion, while AMS can be assessed through both tapping and walking, these tasks differ fundamentally in movement complexity (i.e., fine vs. gross movements), timing-control, and neural mechanisms. The choice of the appropriate target movement can be driven by the research question, while considering the aforementioned differences when designing an experimental protocol. For example, tapping may be more suited to answer questions related to aspects of AMS and timing that can be isolated from whole-body coordination, when minimal motor involvement is needed, or when the focus is primarily on voluntary motor control. There are also pragmatic reasons for choosing tapping over gait. Indeed, walking tasks may be overly challenging for certain individuals, like stroke patients, making tapping a great alternative to assess rhythmic abilities. Alternatively, gait offers

the unique opportunity to study both automatic and voluntary components of motor control. This might be particularly relevant when working with Parkinson's disease patients as walking progressively switches from automatic to attentional control as the disease progresses [110]. Even though testing AMS using gait is certainly more demanding than asking participants to perform a tapping task, gait has the advantage of having high ecological validity and is likely more scalable to everyday life. In the context of rehabilitation, gait tasks can inform on functional deficits linked to autonomy and well-being that cannot be addressed with tapping. Figure 2 summarizes the differences between tapping and walking, which are critical in the design of AMS protocols.

4 | Training Rhythmic Abilities

The links we previously described between beat perception and AMS support the concept of a general rhythm system. This hypothesis suggests that motor benefits for a given effector should increase following training that is focused on another effector (i.e., near transfer) or even nonmotor training (i.e., far transfer). This prospect is particularly relevant for rehabilitating patients with movement disorders who may experience cross-effector benefits from training rhythmic abilities [54]. Beyond movement, rhythmic abilities and music training have been linked to executive functions in healthy individuals [111–113], neurodevelopmental [5–7, 114], and neurodegenerative disorders [115]. For example, children and adults with attention deficit/hyperactivity disorder (ADHD) with greater beat perception and AMS abilities display better performance in cognitive flexibility and inhibition tests compared to those with poorer rhythmic abilities [5]. Cognitive flexibility refers to the ability to adapt behavior to changing task rules [116]. Inhibition involves controlling attention to suppress or delay dominant responses, while working memory refers to the ability to retain and manipulate information [116]. Notably, inhibition control and working memory—both positively correlated with motor production and sensorimotor integration [111, 117]—are crucial aspects of executive functioning. Overall, there is evidence that rhythmic abilities are associated with enhanced cognitive functions. Therefore, training rhythmic abilities may positively influence cognitive performance, which could be particularly beneficial for slowing the cognitive decline associated with normal aging or for supporting individuals with neurological disorders linked to cognitive deficits. In the following section, we first review interventions specifically targeting rhythmic abilities, and then present a discussion of how motor training can enhance both motor and nonmotor skills.

4.1 | Rhythm-Specific Training

Several forms of interventions exist to train rhythmic abilities. The most general form of training is learning to play a musical instrument, which typically includes training rhythmic abilities among other skills. Musicians often outperform nonmusicians on rhythmic tasks [93, 94]. Interestingly, instrumental music training shows transfer effects that go beyond music, probably due to brain-related changes associated with music practice [118]. Although there is currently a debate in the literature regarding the effect of music training on cognitive functions in children [119], growing evidence is in favor of musical interventions, more so than other types of artistic or academic pursuits and sports

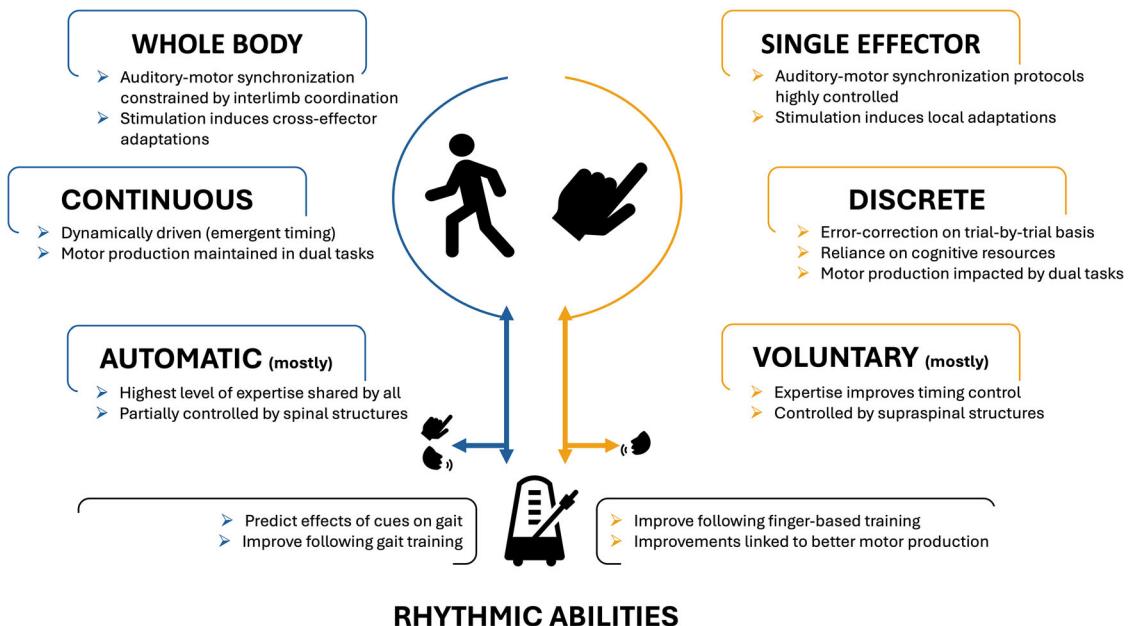


FIGURE 2 | Walking as a model of auditory-motor synchronization compared to finger tapping. Reciprocal arrows indicate effects of rhythmic abilities on motor production and sensorimotor integration, as well as positive impact of gait and finger-based training on rhythmic abilities.

[117, 120–122]. For example, beneficial effects of music training have been shown in inhibition [117] and working memory [120]. Similar results are also observed in older individuals following music training [123–125]. Music interventions are particularly promising for rehabilitation because they are both pleasurable and rewarding [126]. One particularly interesting form of musical activity is drumming. Drumming seems to fall somewhere in-between finger tapping and walking as it can involve all four limbs (on a drum set), requires bilateral coordination, and specifically engages the rhythmic component of music training. Drummers have been shown to outperform other musicians in rhythmic tasks [127], although these differences may be limited to more difficult tasks (i.e., synchronizing to a triple meter) [128]. Notably, drummers often must perform two rhythms independently. They may thus be better at maintaining rhythmic movements [129] while having to perform a secondary task, although motor control remains voluntary during music practice, likely relying on similar neural structures as tapping. Drumming therefore may offer an alternative model for investigating rhythmic abilities and their neural mechanisms, while also opening promising avenues for interventions aimed at enhancing motor coordination and dual-task performance. However, and in spite of all the benefits linked with music practice, music lessons are not always accessible due to barriers such as cost, limited availability of instructors, and transportation requirements. In addition, music practice trains more than just rhythmic abilities, making it difficult to isolate effects of improved rhythmic skills. Therefore, it is essential to explore alternative approaches to training rhythmic abilities that may be more accessible and specifically target rhythmic skills, such as cued-gait training (see Section 4.2) and serious games.

Serious games—designed with goals beyond mere entertainment—can be used for motor rehabilitation in various patient populations (e.g., stroke, Parkinson’s disease, cerebral palsy, etc.) [130], as well as to devise training targeted at rhythmic abilities [131]. These interventions are particularly appealing

because they are affordable, accessible, and can be performed at home with minimal involvement from medical professionals. They may be a suitable alternative for patients with motor disorders for whom learning to play a musical instrument may be too challenging. One example of a serious game designed to enhance rhythmic abilities is *Rhythm Workers* [131], a tablet-based game where users must tap in time with music to construct buildings. After a 6-week training period, individuals with Parkinson’s disease demonstrate improved beat perception compared to those playing a control game [54]. Enhanced beat perception is also linked to improvements in motor production during both manual tasks (i.e., tapping) and verbal tasks (i.e., articulating syllables as fast as possible), suggesting that training rhythmic abilities can transfer to different effectors, regardless of whether they were specifically targeted during training. More recently, this approach was applied to training rhythmic abilities in children with neurodevelopmental disorders. In a pilot study, we found that a 2-week training is effective in improving rhythmic abilities in children with ADHD, relative to an active control condition [114]. Notably, we found first evidence of an improvement of inhibition and flexibility in this clinical population [114]. Although serious games offer a promising approach to enhancing beat perception and motor production, transfer to other effectors is partial, as interstep interval variability did not decrease post intervention [54]. Interestingly, playing *Rhythm Workers* did prevent the increase in interstep interval variability seen in the active control group [54]. Nonetheless, this limited transfer effect may be due to differences in the timing mechanisms employed by various types of movements, as described in the previous section.

4.2 | Gait Training

Another way to implement rhythmic training involves having patients walk with rhythmic cues, such as metronome tones or

music clips, in a rehabilitation program lasting several weeks [132, 133] (for reviews, see Refs. [134, 135]). Locomotion is essential for autonomy and, consequently, for quality of life and well-being [136]. Gait rehabilitation offers the advantage of fostering a functional gain leading to increased independence, while keeping patients physically active during the training itself. Having patients walk on a regular basis over several weeks has been shown to produce positive changes in gait and balance post intervention, even in the absence of cues [137, 138]. The rewarding nature of music [126] makes cued-gait training particularly appealing for motor rehabilitation. Rhythmic auditory cues can induce immediate improvements during walking in Parkinson's disease [16, 76, 139, 140], cerebral palsy [77], and stroke [141], for example. When performed over 3–24 weeks, cued-gait training not only improves gait spatiotemporal parameters immediately post intervention [142–144], but also sometimes after the intervention has ceased [145, 146], though reports are inconsistent [147]. Interestingly, rhythm interventions also enhance rhythmic abilities, namely, beat perception and AMS [10, 148].

Gait has both automatic and voluntary components. Timing involved with voluntary action (e.g., gait initiation, stopping, and turning) can thus transfer to tapping performance and other voluntary motor commands. In contrast, motor gains from rehabilitation designed to focus exclusively on finger movements, such as serious games, may not transfer to full-body, continuous, and automatic movements [54]. Cued-gait rehabilitation may thus train rhythmic abilities more broadly than finger-tapping-based interventions.

One way to implement cued-gait training is by using technologies that adapt stimulus-presentation rate to individual cadences. These technologies have shown positive effects on gait (e.g., speed increase) in neurotypical and patient populations [149–151]. Such technologies can provide metronome cues that match individuals' preferred cadence in order to facilitate gait, but can also provide gradual tempo changes, which could be harnessed to train beat perception, AMS and gait itself in an enjoyable fashion. Cochen De Cock et al. tested effects of such intervention on Parkinson's disease patients with BeatMove, which provides musical stimuli synchronized to participants footsteps with gradual tempo changes to elicit faster cadence. After a 4-week intervention, patients improved not only spatial and temporal gait parameters, but also overall physical activity and reported satisfaction with the device [152]. These results are very promising for the design of personalized gait interventions for patients with movement disorders.

In sum, training rhythmic abilities can lead to benefits in motor and cognitive performance. Cued-gait interventions may be ideal to train rhythmic skills more broadly, as gait has both automatic and voluntary components that can transfer to other movements. Gait also has the advantage of being functional, since it facilitates autonomy and keeps patients physically active. Combining music cues with gait training will make interventions more enjoyable and rewarding. Alternatively, music lessons and specifically drum lessons, may lead to similar benefits. Future studies comparing near- and far-transfer effects following cued-gait, serious games and drum interventions are needed.

5 | Practical Implications and Challenges for Testing Gait

Assessing AMS using gait may seem challenging without access to expensive motion capture systems or instrumented treadmills, typically found in biomechanics laboratories. Additionally, using brain-imaging techniques during gait, such as electroencephalography (EEG) or functional near-infrared spectroscopy (fNIRS), may seem arduous due to their sensitivity to motion artifacts. In this section, we offer practical ways to implement gait paradigms using equipment that can be found in music cognition laboratories and protocols that can be easily devised with sets of sensors and microcontrollers (e.g., Arduino-based).

Data collection in tapping experiments often relies on force signals from force sensitive resistors (FSRs) to extract tap events. An example is the TeensyTap device [153], in which an FSR is connected to a teensy microcontroller board (PJRC, Portland, Oregon, USA), coupled to an audio extension shield to record tap data while providing auditory stimulation. Our team recently adapted this technology to gait with TeensyStep [150], offering a cheap and portable alternative to construct flexible AMS paradigms during locomotion while keeping high level temporal precision. Codes for TeensyTap (<https://github.com/florisvanvugt/teensytap>) and TeensyStep (<https://github.com/dallabella-lab/teensystep>) are open source and can be easily adapted to a researcher's interests. Using FSRs rather than motion capture systems or instrumented force plates also facilitates the transfer of AMS protocols to both ecological (i.e., outside the lab) and clinical settings, as equipping patients with reflective markers or a harness may be suboptimal.

Studying gait at the neural level requires portable devices such as EEG and fNIRS. One drawback of these devices is their sensitivity to motion artifacts inherent to walking tasks [154–156]. Nonetheless, multiple algorithms have now been developed to improve signal-to-noise ratio [154], such as the BeMoBIL pipeline [157], leading to an increasing number of gait publications in the last two decades [158–160].

Together, these cost-effective and accessible hardware and software developments pave the way for assessment of gait and its neural underpinnings in the context of AMS research.

6 | Conclusion and Perspectives

Finger tapping has significantly contributed to our understanding of AMS due to its simplicity and ease of use in both the laboratory and at home. It serves as a reliable proxy for assessing AMS in research and clinical settings when time and equipment is limited. However, finger tapping is a single effector, discrete, and mostly voluntary movement which timing heavily relies on cognitive resources and structures. Tapping is a relatively unstable motor behavior that is difficult to sustain while simultaneously performing other cognitive or motor tasks. Consequently, assessing motor production and AMS using only the finger may provide an incomplete picture of one's rhythmic profile. Moreover, findings from finger-tapping tasks may not translate well to other types of movements such as walking.

Despite the greater difficulty in testing and measuring gait performance, walking offers a more comprehensive perspective on rhythmic abilities. It involves the coordination of multiple effectors, is continuous, and is largely automatic. Gait training can improve all dimensions of rhythmic abilities, including beat perception, motor production, and sensorimotor integration. Additionally, recent technological advancements such as Mobile Brain/Body Imaging (MoBI) [161] have made it possible to investigate more naturalistic movements, like walking, even at the cortical level. This progress allows researchers to move beyond highly controlled environments to study rhythmic abilities through truly rhythmic motor actions.

Studies are now needed to directly compare finger tapping and walking across various paradigms (e.g., spontaneous movements, synchronization, dual tasking) to better understand differences in timing-control mechanisms. Comparing different types of interventions across diverse populations will also be essential for refining the concept of a generalized rhythm system and developing patient-specific rehabilitation protocols.

Author Contributions

Both authors discussed and agreed on the conception of the manuscript and its main topics. They both contributed to the writing and approved the final version for publication.

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Conflicts of Interest

The authors declare no conflicts of interest.

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